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Solving the interior problem of computed tomography using *a priori* knowledge

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Abstract

A case of incomplete tomographic data for a compactly supported attenuation function is studied. When the attenuation function is *a priori* known in a subregion, we show that a reduced set of measurements are enough to uniquely determine the attenuation function over all the space. Furthermore, we found stability estimates showing that reconstruction can be stable near the region where the attenuation is known. These estimates also suggest that reconstruction stability collapses quickly when approaching the set of points that is viewed under less than 180°. This paper may be seen as a continuation of the work 'Truncated Hilbert transform and image reconstruction from limited tomographic data' (Defrise *et al* 2006 *Inverse Problems* 22 1037). This continuation tackles new cases of incomplete data that could be of interest in applications of computed tomography.

1. Introduction

In two-dimensional (2D) computed tomography (CT), all line integrals of the attenuation function may not always be available. When all line integrals are available, there is an accurate and stable reconstruction formula to recover the attenuation function from the measurements [15, 22]. But when the set of measurements is not complete, several problems can arise. Different complications appear depending on how the data set is truncated. In textbooks, the kinds of possible truncations are generally listed into three distinct classes: the limited angle problem, the exterior problem and the interior problem. Below we briefly review these three problems and then focus the discussion on the interior problem, for which we present here new theoretical results. First, let us clarify that we consider a continuum of measurements, and when we talk about truncation of the data set we are not thinking about discretization of the measurements, but about limitation of the measurements in this continuous

setting. Let us also mention that when we talk about measured lines, measured data or just measurements, this is a slight abuse of language. The line integral of the attenuation function is not equal to the intensity of the x-ray beam measured at the detector, but we call them measured data because they are computed automatically from the intensity measured at the detectors.

Various acquisition geometries can be used to measure the line integrals. For example, early CT scanners used the parallel-beam geometry while the fan-beam geometry is now preferred. In any case, a simple reparametrization always allows a description of the measured line integrals using the Radon transform notation. We adopt this notation. Let $\mu(x)$ be the attenuation function to be reconstructed. We parameterize the lines in \mathbb{R}^2 with an angle α and a scalar $s \in \mathbb{R}$, and we let the line integral along the (s, α) line be $R\mu(s, \alpha)$. The angle α defines the direction of the line, while s specifies the signed distance from the origin to the line. This distance is measured in the direction of vector $\theta(\alpha) := (\cos \alpha, \sin \alpha)$, and $\theta^{\perp}(\alpha) := (-\sin \alpha, \cos \alpha)$, which is obtained by rotating θ counterclockwise by 90° , is the line direction. By construction,

$$R\mu(s,\alpha) := \int_{\mathbb{R}} \mu(s\theta(\alpha) + t\theta^{\perp}(\alpha)) dt.$$

Observe that $R\mu(s,\alpha)=R\mu(-s,\alpha+\pi)$ since (s,α) parameterizes the same line as $(-s,\alpha+\pi)$. Also observe, for a similar reason, that $R\mu(s,\alpha)=R\mu(s,\alpha+2k\pi)$ for any integer k.

To describe the region covered by the object being scanned, we use the concept of support of a function. The support of the attenuation function $\mu(x)$ is defined as the smallest closed set outside which the attenuation function vanishes. To keep the arguments simple, we may not distinguish between the support of the attenuation function and the region covered by the object, though this requires the attenuation function to be non-zero inside the object.

We now review the limited angle problem, the exterior problem and the interior problem. The limited angle problem appears when knowledge of the Radon transform $R\mu(s,\alpha)$ is restricted to the set $(s,\alpha) \in \mathbb{R} \times [-\phi,\phi]$ with $\phi < \pi/2$. This situation arises, for example, in electron microscopy or radio astronomy, where the angle of view is restricted. In the case of the limited angle problem, the data are enough to uniquely determine the attenuation function (e.g. [22]). However, the inversion is severely ill-posed and it is not possible to obtain a good reconstruction of the attenuation function in presence of data noise. This fact is emphasized by the singular value decomposition of the limited-angle Radon transform [19].

The exterior problem arises when the Radon transform is only measured over the lines that do not intersect a ball of radius a. In other words, $R\mu(s,\alpha)$ is known only on the (s,α) lines defined with |s| > a. This situation happens in non-destructive material testing. For instance, it is of special interest to detect cracks or corrosion in the outermost layers of pipes and rockets. X-ray CT is a way to achieve this task, but the object is in general so dense that x-rays cannot cross through the diameter, and therefore only exterior measurements can be obtained. In the case of the exterior problem, the measurements are enough to uniquely determine the attenuation function for the points satisfying |x| > a (Helgason's support theorem, [15]), and a reconstruction formula for these points was provided by Cormack [6]. But, as shown by singular value decomposition [25], the exterior problem is also very ill-posed, so that accurate reconstruction of the attenuation function is hardly possible from real (noisy) data.

The interior problem appears when we measure only the line integrals that intersect a ball totally contained inside the object. Namely, the Radon transform is available only for the lines intersecting the set FOV := $\{x \in R^2 : |x| < a\}$ and this set is inside the object (FOV stands for field of view). This situation could appear in medical imaging when we are interested in reconstructing the attenuation function only in a region of interest (ROI). Indeed, in such a

case, it is desirable to reduce the patient exposure to x-ray radiation by measuring only the line integrals that go through that region. In general, such a set of measurements are not enough to uniquely determine the attenuation function, not even inside the FOV. Nonetheless, the undetermined part is not arbitrary [14]; it belongs to a space of functions which are smooth in the set |x| < a. A singular value decomposition of this problem, for the fan-beam and parallel-beam geometries, can be found in [20, 21].

In summary, truncation of the data set strongly impacts the CT reconstruction problem. It either eliminates the possibility of recovering the value of the attenuation function (interior problem) or makes the reconstruction of the attenuation function very unstable (limited angle and exterior problems). Such a behavior, in addition to the non-local nature of the classical inversion formula for the 2D Radon transform [15, 22], sustained the belief that in two dimensions, reconstruction at a given point required knowledge of the transform over all possible lines in order to be accurate and stable.

There exist some insightful results about what can be stably recovered from local data. More specifically, it is known that limited sets of measurements can be enough to reconstruct the singularities of the attenuation function in a stable way [13, 16, 26]. By singularities of the attenuation function we mean, for example, discontinuities of the function. To be able to determine in a stable way a discontinuity of the attenuation function at a given point, knowledge of all line integrals through a neighborhood of that point is required. In particular, this means that for the limited angle problem and the exterior problem, there are discontinuities that cannot be detected in a stable way. On the other hand, in the interior problem, there are enough data to recover the discontinuities of the function inside the ball $\{x \in \mathbb{R}^2 : |x| < a\}$ (i.e. inside the FOV). The relation between the singularities of a function and the singularities of its Radon transform, and stability estimates in Sobolev spaces, can be found in [13, 26].

Summarizing, the number of measurements in the interior problem is enough to recover the discontinuities of the function inside the FOV, but not enough to determine the value of the function at any point. Surprisingly, this situation changes drastically when the FOV is not completely contained inside the object. We elaborate on this change below.

Assume that $R\mu(s,\alpha)$ is measured for all lines intersecting FOV = $\{x \in \mathbb{R}^2 : |x| < a\}$. Assume that the FOV is not completely contained inside the object. Assume that the attenuation function $\mu(x)$ is continuously differentiable and with known compact support, i.e. $\mu(x)$ vanishes outside some compact set and we know that set. In such a case, when the object is convex and the FOV contains opposite sides of the boundary, some recent papers have provided accurate inversion formulae for the attenuation function in a subregion of the FOV (e.g. [4, 5, 23, 24, 31–35]). Some non-convex objects, such as that in figure 3(a), are also covered by these results. These inversion formulae are semi-local: knowledge of line integrals far from the reconstruction point are still necessary, but it is not required to know *all* the line integrals. It is important to observe that, on one hand, we allow considerable truncation in the set of measurements. But on the other hand, for reconstruction to be possible, we require some extra *a priori* knowledge on the location and support of the object. Note that the required extra knowledge is far from being equivalent to having complete measurements. In particular, it does not imply that accurate reconstruction of the attenuation function, or its discontinuities, is possible outside the FOV [13, 26].

Most of the semi-local inversion formulae cited in the above paragraph require the FOV to contain opposite sides of the boundary of the object (as in figure 3(a)). Interestingly, some useful results can also be stated in the case where the FOV exceeds the object only from one side (as in figure 3(b)). Indeed, it was proved in [11] that, in such a case, the data are still enough to uniquely determine the attenuation function inside the FOV. Moreover, a

pointwise stability result was found. This stability result suggests that reconstruction of the attenuation function should be more stable for the FOV points that are near the boundary of the object, and that reconstruction stability may logarithmically decrease as we go deeper into the object.

In the present paper, we focus on the interior problem. This means that we assume knowledge of the Radon transform for all lines intersecting the FOV = $\{x \in \mathbb{R}^2 : |x| < a\}$ and that we allow this field of view to be completely contained inside the object. However, unlike other studies on the interior problem, we include some extra *a priori* knowledge: we assume that the compact support of the attenuation function is known, and we also assume that the value of the attenuation function is known in some subregion of the FOV. Under these hypotheses, we extend the uniqueness and stability results of [11] to new cases of practical interest. Such extensions provide tools to explore image reconstruction in truncated CT and can translate into a reduced radiation dose in CT, which is becoming of increasing importance as well described in the introduction of [29].

Uniqueness results for the interior problem with prior knowledge have been obtained in our earlier work [17, 18] and independently in [29]. The result presented here is slightly stronger in concluding uniqueness over the whole space instead of just a restricted region. Uniqueness however does not imply stability, and therefore the main focus of the present paper is a theoretical analysis of stability. In [17, 18, 29], the good stability of this inverse problem was demonstrated empirically for specific reconstruction algorithms, which use the POCS (projection on convex sets) method to invert the Hilbert transform with limited data. Although POCS is an efficient algorithm with guaranteed convergence if the data are noise-free (consistent), it does not by itself guarantee stability when applied to ill-posed problems with noisy data, such as, for instance, the severely ill-posed problem of limited-angle tomography. This motivated a theoretical analysis of the stability of the interior problem with prior knowledge, which led us to point-wise upper bounds on the reconstruction error that are independent of the specific algorithm used for reconstruction, as soon as this algorithm enforces a number of constraints. These results (theorems 4.2 and 4.3) are useful since they show that the problem is not arbitrarily unstable and they give insight into the accuracy that is attainable. We will also present some numerical examples with simulated data to illustrate the theoretical results, using the same POCS algorithm as in [18]. We refer the reader to [18] for a detailed numerical study for a variety of geometric configurations, and with different sets of prior knowledge, some of which are not covered by the results included here. The results here, together with the studies already done in [18, 29, 30], point out new interesting data acquisition settings, where accurate and stable reconstruction may be possible.

The organization of the paper is as follows. Section 2 contains background material on mathematical concepts; specifically, we review the definition and properties of the Hilbert transform and Nevanlina's principle. These tools will be essential in the following sections. In section 3, we recall the differentiated backprojection (DBP) formula that relates the Radon transform and the directional Hilbert transform, the formula that together with the inversion of the truncated Hilbert transform produces the semi-local inversion formulae presented in papers [23, 24]. In section 4, we describe explicitly the interior problem with *a priori* knowledge (figures 4 and 5). We also analyze the implications of the results presented in previous sections, and with some extra calculation, we obtain the main uniqueness and stability results of this paper. In particular, in section 4 we use the relation presented in section 3 to reduce the problem of inverting the Radon transform in 2D to a problem on the Hilbert transform in 1D. In section 5, numerical experiments are done in order to support the theoretical results of section 4. Section 6 mentions possible extensions, in particular to the 2D fan-beam and the 3D cone-beam geometries. Section 7 contains the conclusions.

2. Background material

2.1. Hilbert transform on the real line

Unless otherwise specified, all over this section f is going to be a function in $C_0^{\sigma}(\mathbb{R})$ with $0 < \sigma \le 1$ (see appendix A).

For a function $f \in C_0^{\sigma}(\mathbb{R})$, its Hilbert transform is a function in $C^{\sigma}(\mathbb{R})$ defined as

$$\mathrm{H}f(y) := \frac{1}{\pi}\mathrm{p.v.}\int_{\mathbb{R}}\frac{f(x)}{x-y}\,\mathrm{d}x := \frac{1}{\pi}\lim_{\epsilon\to 0}\Bigg[\int_{-\infty}^{y-\epsilon}\frac{f(x)}{x-y}\,\mathrm{d}x + \int_{y+\epsilon}^{\infty}\frac{f(x)}{x-y}\,\mathrm{d}x\Bigg].$$

Since $\frac{1}{x-y}$ is not integrable at x=y, to make sense of the integral it is necessary to remove a ball of radius ϵ around y and then let $\epsilon \to 0$. This is defined as the Cauchy principal value of the integral, and it is denoted with a p.v.

The Hilbert transform is a classical transformation that appears in many different subjects, in particular it relates the real and imaginary parts of analytic complex-valued functions. It satisfies H(Hf)(x) = -f(x) and it also verifies the following property.

Lemma 2.1. Let (a, b) be any non-empty open interval in \mathbb{R} . If f(x) = 0 and Hf(x) = 0 for $x \in (a, b) \subset \mathbb{R}$, then $f \equiv 0$ in \mathbb{R} .

Proof. Let $\Omega = (\mathcal{C} \setminus \mathbb{R}) \cup (a, b)$, i.e. Ω is the complex plane with the intervals $(-\infty, a)$ and (b, ∞) removed. For $z \in \Omega$, define

$$g(z) := \frac{1}{\pi} \left[\int_{-\infty}^{a} \frac{f(x)}{x - z} dx + \int_{b}^{\infty} \frac{f(x)}{x - z} dx \right].$$

The function g(z) is analytic in Ω and satisfies the classic Plemelj–Sokhotski formula [1, 2]: for any $x \in \mathbb{R} \setminus [a, b]$,

$$\lim_{y \to 0^+} g(x + iy) - \lim_{y \to 0^-} g(x + iy) = \frac{1}{2i} f(x).$$

We assumed that $f \equiv 0$ in (a, b); hence, from its definition, g(x) = Hf(x) for $x \in (a, b)$. But we additionally assumed that Hf(x) = 0 in (a, b). Therefore, $g \equiv 0$ in (a, b) and consequently the analyticity of g implies $g(z) \equiv 0$ all over Ω . Using this and the Plemelj–Sokhotski formula, we obtain that f(x) = 0 for any $x \in \mathbb{R} \setminus [a, b]$. Since we had already assumed that f(x) = 0 in (a, b), the continuity of f implies that $f \equiv 0$ on all of \mathbb{R} .

Corollary 2.2. For any non-empty interval (a, b), knowledge of f(x) and Hf(x) for all $x \in (a, b)$ uniquely determines the value of f over all the real line.

The next result about the Hilbert transform is quite remarkable [27, 28], and this property will be referred to as the inversion formula for the truncated Hilbert transform. For simplicity, suppose that the support of a given function f is contained in the interval (-1, 1). The knowledge of the Hilbert transform in (-1, 1), plus some small a priori knowledge on f, is enough to recover the function with the following inversion formula.

Theorem 2.3. Let f be such that its support set is contained in (-1, 1) and assume that g(x) = H f(x) is known in that interval. Then, for $x \in (-1, 1)$,

$$\sqrt{1-x^2}f(x) = C + \frac{1}{\pi} \text{p.v.} \int_{-1}^1 \frac{g(y)}{x-y} \sqrt{1-y^2} \, dy,$$

where C is a constant to be determined by a priori knowledge on f. For example, under the current assumptions, C can be determined by using the relation $C = \frac{1}{\pi} \int_{\mathbb{R}} f(x) \, dx$ or from knowing some $\epsilon > 0$ for which f(x) = 0 for $x \in (-1, -1 + \epsilon) \cup (1 - \epsilon, 1)$.

2.2. Nevanlina's principle

Apart from the Hilbert transform, the other important result we will use is known as Nevanlina's principle [2]. It provides an upper bound for the modulus of analytic functions and will be later used to estimate errors in the reconstruction of the attenuation function.

Nevanlina's principle will be used in the following context. Consider $\Omega \subset \mathcal{C}$ to be a connected open subset of the complex plane with a piecewise smooth boundary. The boundary of Ω is the points that delimit Ω from its complement and it is denoted as $\partial\Omega$. A real-valued function $\omega(z)$ is said to be harmonic in Ω if the Laplacian of the function vanishes in the domain, i.e. if $\Delta\omega(z)=0$ for all z in Ω . A harmonic function in Ω satisfies the maximum principle; this means that it attains its maximum and minimum values on the boundary of Ω .

Theorem 2.4. Let f(z) be an analytic function in a domain $\Omega \subset \mathcal{C}$. Let $D \subset \partial \Omega$ be a segment of the boundary. Let $\omega(z)$ be a harmonic function in Ω satisfying

$$\omega(z) = \begin{cases} 0 & \text{for } z \in D \\ 1 & \text{for } z \in \partial \Omega \backslash D \end{cases}$$

$$|f(z)| \leq \begin{cases} \epsilon & \text{for } z \in D \\ M & \text{for } z \in \partial \Omega \backslash D, \end{cases}$$

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$$|f(z)| \leq \begin{cases} \epsilon & \text{for } z \in D \\ M & \text{for } z \in \partial \Omega \backslash D, \end{cases}$$

then

$$|f(z)| \le M \left(\frac{\epsilon}{M}\right)^{1-\omega(z)}$$
 for all $z \in \Omega$. (2.1)

Because of the maximum principle, $\omega(z)$ depends only on the domain Ω and the set $D \subset \partial \Omega$. Also, $0 < \omega(z) < 1$ for $z \in \Omega$. This harmonic function is called Nevanlina's exponent for Ω and D.

2.3. Applying Nevanlina's principle

Consider a disk in the complex plane. Remove from this disk a segment of its horizontal diameter, as shown in figure 1, and let that domain be Ω . We picture the diameter as being the interval (a,c) of the real line, while the removed segment is the interval (b,c). We let D=(b,c) so that $\partial\Omega\setminus D$ is the boundary of the disk. These Ω and D are the particular case in which we will apply Nevanlina's principle, so let us compute Nevanlina's exponent explicitly for such a domain.

The easiest way to compute the exponent is to map Ω conformally into the upper half-plane $\{z \in \mathcal{C} : \operatorname{Im}(z) > 0\}$, mapping D onto the interval $(0, \infty)$. Once in the upper half-plane an expression for Nevanlina's exponent is straightforward. Indeed, if z_5 is a point in the upper half-plane, write it as $z_5 := r \operatorname{e}^{\mathrm{i}\beta}$ with r > 0 and $\beta \in (0, \pi)$. The function $\omega_H(r \operatorname{e}^{\mathrm{i}\beta}) = \beta/\pi$ happens to be harmonic, bounded and takes the values 0 on $(0, \infty)$ and 1 on $(-\infty, 0)$.

We map Ω onto the upper half-plane by using a sequence of conformal maps. In figure 1 we show the intermediate domains that we map through, keeping track of the images of the sets D (dark solid line), $\partial \Omega \setminus D$ (thin solid line) and $(a, b) \subset \Omega$ (dark dotted line). The conformal maps that we use, and a short description of what they do, are as follows.

• Translation and scaling of the disk, centering the disk at 0 and normalizing the radius:

$$z_1: z \mapsto \frac{z - \left(\frac{a+c}{2}\right)}{\frac{c-a}{2}}.$$

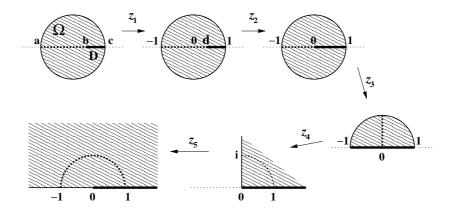


Figure 1. Sequence of conformal maps from Ω to the upper half-plane. The images of D correspond to the dark solid line. The images of $\partial\Omega\backslash D$ correspond to the thin solid line. The images of the interval $(a,c)\subset\Omega$ correspond to the dark dotted line.

• Linear fractional transformation that maps $d \mapsto 0$, while mapping the disk onto itself:

$$z_2: z \mapsto \frac{z-d}{1-\bar{d}z}$$
 for $d = \frac{2b-a-c}{c-a}$.

• A duplicated D is mapped onto (-1, 1), mapping the disk to a half-disk. This is achieved by using a square root with a branch along $[0, \infty)$:

$$z_3: z \mapsto \sqrt{z}$$
.

• Linear fractional transformation that maps the half-disk to a quadrant of C:

$$z_4: z \mapsto \frac{1+z}{1-z}.$$

• Open the quadrant onto the upper half-plane:

$$z_5: z \mapsto z^2$$
.

Summarizing, we map Ω conformally onto the upper half-plane using the composition of maps $z_5 \circ z_4 \circ z_3 \circ z_2 \circ z_1$, mapping D onto $(0, \infty)$ and $\partial \Omega \setminus D$ onto $(-\infty, 0)$. Once in the upper half-plane we compose with ω_H to obtain Nevanlina's exponent for Ω , D. Therefore, Nevanlina's exponent for Ω , D can be computed as $\omega(z) := \omega_H(z_5(z_4(z_3(z_2(z_1(z))))))$. Though this is a rather complicated expression, it is not hard to compute w(z) explicitly for $z \in (a,b)$, noting that $(a,b) \subset \Omega$ is mapped onto $\{z: |z| = 1, \operatorname{Im}(z) > 0\}$ in the upper half-plane.

Lemma 2.5. For the domain $\Omega \subset \mathcal{C}$ specified above and D = (b, c), Nevanlina's exponent at $x \in (a, b)$ has the following expression:

$$\omega(x) = -\frac{4}{\pi} \arctan \sqrt{\frac{2(b-x)(c-a)}{(c-a)^2 - (2b-a-c)(2x-a-c)}}.$$
 (2.2)

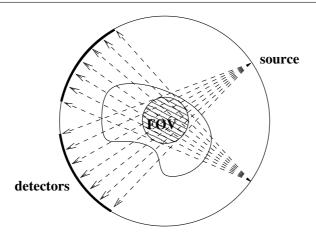


Figure 2. Typical data acquisition setting in x-ray CT. The source and detectors rotate around the patient. The shadowed region represents the FOV.

3. Differentiated backprojection and Hilbert transform

In computerized tomography, the goal is to reconstruct an unknown attenuation function from some of its line integrals. In the absence of noise, these line integrals correspond exactly to the measured data. In modern scanners, the data are acquired by an x-ray source and detectors rotating around the patient (see figure 2). In such a setting, the measured data give rise to the concept of FOV: the set of points through which the line integrals in all directions are measured. This FOV corresponds exactly to our previous definition FOV := $\{x \in \mathbb{R}^2 : |x| < a\}$ (e.g. figure 2). Recalling the definition of $R\mu(s,\alpha)$ from the introduction, the FOV corresponds to the set of points in \mathbb{R}^2 for which $R\mu(x \cdot \theta(\alpha), \alpha)$ is known for all $\alpha \in [0, \pi)$. Here, $x \cdot \theta$ denotes the inner product in \mathbb{R}^2 . We will refer to the region outside the FOV as the region of incomplete measurements since for $x \notin \text{FOV}$, $R\mu(x \cdot \theta(\alpha), \alpha)$ is known only for α in an angular range smaller than $[0, \pi)$.

Consider a function $\mu \in C_0^{\infty}(\mathbb{R}^2)$ and fix a vector $\eta \in \mathbb{R}^2 \setminus \{0\}$. The Hilbert transform of μ in the direction η at point $x \in \mathbb{R}^2$ is defined as

$$H_{\eta}\mu(x) := -\frac{1}{\pi} p.v. \int_{\mathbb{R}} \frac{\mu(x - t\eta)}{t} dt.$$

This is an odd function in η , namely $H_{-\eta}\mu(x) = -H_{\eta}\mu(x)$.

For an attenuation function μ , the connection between its Radon transform and this Hilbert transform is as follows [23].

Lemma 3.1. Let θ_1, θ_2 and $\theta(\alpha)$ be the unitary vectors corresponding to α_1, α_2 and α respectively, where α_1 and α_2 are arbitrary angles and $\alpha \in \left[\alpha_1 - \frac{\pi}{2}, \alpha_2 - \frac{\pi}{2}\right]$. Then

$$-\frac{1}{\pi} \int_{\alpha_1 - \frac{\pi}{2}}^{\alpha_2 - \frac{\pi}{2}} \left[\frac{\partial}{\partial s} R \mu(s, \alpha) \right]_{s = x \cdot \theta(\alpha)} d\alpha = H_{\theta_2} \mu(s) - H_{\theta_1} \mu(s). \tag{3.1}$$

Since the directional Hilbert transform is odd in η , we get the following corollary.

Corollary 3.2. Let θ_0 be the unitary vector corresponding to α_0 . Then

$$\frac{1}{2\pi} \int_{\alpha_0 - \frac{\pi}{2}}^{\alpha_0 + \frac{\pi}{2}} \left[\frac{\partial}{\partial s} R \mu(s, \alpha) \right]_{s = x \cdot \theta(\alpha)} d\alpha = H_{\theta_0} \mu(x). \tag{3.2}$$

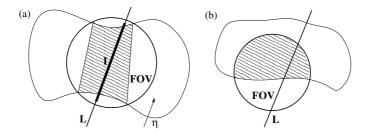


Figure 3. (a) Not all line integrals are measured, but $\mu(x)$ can be reconstructed in the shadowed region. (b) The attenuation $\mu(x)$ is uniquely determined in the shadowed region.

This formula relates the Radon transform and the Hilbert transform over a line. It will be used to reduce the problem of inverting the Radon transform in 2D to the problem of inverting the Hilbert transform in 1D. Corollary 3.2 implies the following for the points in the FOV.

Corollary 3.3. For a point x in the FOV and in the case of noiseless measurements, $H_{\eta}\mu(x)$ can be computed from the measured data for any direction η .

Let us study the consequences of the previous result. In particular, let us revisit some of the results presented in [11, 23].

Assume that we have the situation of figure 3(a): the object is described by the thin line and we know the boundary of the object. The circle represents the FOV and therefore we measure all the line integrals intersecting that circle. As in figure 3(a), pick a line L that exits the object at opposite sides contained in the FOV. Let η denote the direction of such a line. Corollary 3.3 tells us that from the measurements, we can compute $H_{\eta}\mu(x)$ for all points x in $L \cap FOV$. This includes a segment $I \subset L$ such that $\mu(x) = 0 \ \forall x \in L \setminus I$. As we will see in more detail in section 4, in such a setting the inversion formula for the truncated Hilbert transform (theorem 2.3 in this paper) allows us to recover $\mu(x)$ over the line L. Using the same argument over different lines, we obtain an inversion formula for all the points in the shadowed region of figure 3(a). This is essentially the inversion formula presented in [23].

A key element in the previous argument is that the FOV needs to be large enough, and be located in such a way with respect to the object, that it covers opposite portions of the boundary of the object. Therefore, the previous argument does not work anymore when the FOV only covers one side of the object, as that in figure 3(b). We can still consider a line L that, at least in one direction, exits the object at a piece of boundary contained in the FOV. We can compute $H_{\eta}\mu(x)$ for all points x in $L \cap FOV$, but there are points in L where $\mu(x)$ does not vanish and where we are not able to compute $H_{\eta}\mu(x)$. Still, in [11] it is proved that the measured data are enough to uniquely determine $\mu(x)$ inside the FOV. Additionally, some stability estimates are provided about how the non-measured data influence the inversion of the Hilbert transform at points in the FOV. Theorem 4.2 in this paper is an extension of the estimates in [11]. In this paper we also present a generalization of the uniqueness result of [11], showing that, actually, the measurements in figure 3(b) determine the function $\mu(x)$ uniquely over all the object, although may be not stably everywhere. This is a consequence of lemma 2.1 and corollary 3.3, and will be presented in detail in the following section.

The situation described in figure 3 arises in medical imaging when the patient is bigger than the FOV or when we want to reduce the size of the FOV to reduce the patient exposure to x-ray radiation.

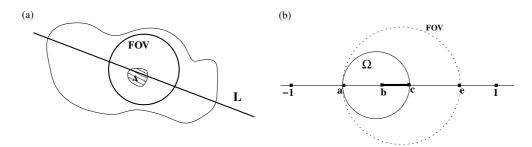


Figure 4. (a) The attenuation function is known *a priori* in region *A*. (b) In reduction to 1D, region *A* correspond to the interval (b, c); therefore, f(t) is known in that interval. The FOV corresponds to the interval (a, e); therefore, Hf(t) can be computed from the measured data inside the interval (a, e).

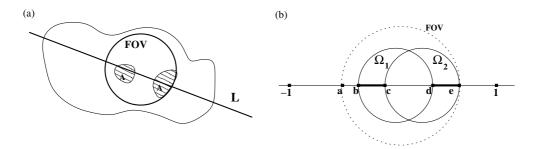


Figure 5. (a) The attenuation function is known *a priori* in region *A*. (b) In reduction to 1D, region *A* corresponds to the intervals $(b, c) \cup (d, e)$.

4. Incomplete data and a priori knowledge

We are now ready to present the case studied in this paper. As mentioned in the introduction, we consider the interior problem: we assume that the FOV is completely contained inside the object. In order to tackle the problem, we assume that we know the boundary of the object and that we know the value of the attenuation function in a subregion A inside the FOV. This situation is represented in figures 4(a) and 5(a).

First, we study the situation described in figure 4(a). For such a case we are able to obtain uniqueness and stability result, presented in corollary 4.1 and theorem 4.2 respectively. Later, we focus on the situation described in figure 5(a). The analysis will be analogous and the uniqueness result applies immediately, but we obtain a somewhat stronger stability result for the points in the FOV that are between regions where $\mu(x)$ is assumed to be known (theorem 4.3).

The uniqueness result establishes that the truncated measurements and the *a priori* knowledge are enough to determine the attenuation uniquely. For this result to hold, we also need to assume that the measurements are noiseless and, therefore, that they correspond exactly to $R\mu(s,\alpha)$.

4.1. Reducing to a 1D problem

Consider a line L that intersects the region A as in figure 4(a). We regard the function $\mu(x)$ restricted to the line L. For that, fix $x_0 \in L$ and choose $\eta \in \mathbb{R}^2 \setminus \{0\}$ such that

 $L = \{x_0 + t\eta : t \in \mathbb{R}\}$. For $t \in \mathbb{R}$, define $f(t) := \mu(x_0 + t\eta)$. Such a function corresponds to the restriction of $\mu(x)$ to the line L and from its definition $f \in C_0^{\infty}(\mathbb{R})$. We also have the following relation between the Hilbert transform of f(t) and the directional Hilbert transform of $\mu(x)$:

$$H f(t_0) = \frac{1}{\pi} p.v. \int_{\mathbb{R}} \frac{f(s)}{s - t_0} ds = \frac{1}{\pi} p.v. \int_{\mathbb{R}} \frac{f(s + t_0)}{s} ds$$

$$= \frac{1}{\pi} p.v. \int_{\mathbb{R}} \frac{\mu(x_0 + (s + t_0)\eta)}{s} ds = \frac{1}{\pi} p.v. \int_{\mathbb{R}} \frac{\mu(x_0 + t_0\eta + s\eta)}{s} ds$$

$$= -H_{-\eta} \mu(x_0 + t_0\eta)$$

$$= H_{\eta} \mu(x_0 + t_0\eta).$$

Therefore, if $(x_0 + t_0 \eta) \in FOV$ corollary 3.3 implies that $H_{\eta}\mu(x_0 + t_0 \eta)$ can be computed from the measured data; hence, $H f(t_0)$ can be computed from the measured data. In addition to that, if $(x_0 + t_0 \eta) \in A$ then $\mu(x_0 + t_0 \eta)$ is assumed to be known; hence $f(t_0)$ is known.

This idea is summarized in figure 4. The function μ restricted to the line L corresponds to a function $f: \mathbb{R} \to \mathbb{R}$. The FOV corresponds to an interval (a, e) and perfect measurement of $R\mu$ for the lines intersecting the FOV translate, using formula (3.2), into the knowledge of Hf(t) for $t \in (a, e)$. The region $A \subset FOV$ corresponds to an interval $(b, c) \subset (a, e)$ and knowledge of $\mu(x)$ for $x \in A$ translates into knowledge of f(t) for $t \in (b, c)$.

In particular, using corollary 2.2, this implies that f is uniquely determined over \mathbb{R} and the following result follows.

Corollary 4.1. We recall that $\mu(x) \in C_0^{\infty}(\mathbb{R}^2)$. If $\mu(x)$ is known in a non-empty open region A contained in the FOV and the measurements are noiseless, then μ is uniquely determined over all lines L intersecting A. This readily implies that μ is uniquely determined in \mathbb{R}^2 .

The above reduction of the original problem to a 1D problem is quite useful. The problem of recovering μ over $L \cap FOV$ reduces to recovering f(t) in the interval (a, e) (see figure 4). The information that is available to us to reconstruct f(t) comes from the *a priori* knowledge on $\mu(x)$ and the measurements of $R\mu(s,\alpha)$. We established that perfect measurement of $R\mu(s,\alpha)$ for the lines intersecting the FOV implies that μ is uniquely determined. Now we will study what happens when we allow errors in the measurements.

In the presence of noise the measurements are not exactly $R\mu(s,\alpha)$ anymore, and we denote them as $R_m\mu(s,\alpha)$. For a given line L, we can compute the left-hand side of the DBP formula by using $R_m\mu(s,\alpha)$ instead of $R\mu(s,\alpha)$ (equation (3.2)) and then restrict the problem to 1D as we did above. We denote by $g_m(t)$ the function obtained using the prescribed procedure. If the measurements were perfect, the DBP formula tells us that $g_m(t) = Hf(t)$, but in the presence of noise this need not be the case.

4.2. Setting of the problem

In this subsection and the following ones, the variable x will denote a point in \mathbb{R} , as in section 2. This is for simplicity of notation when doing references to complex variables.

Let us assume without loss of generality that supp $f \subset (-1, 1)$. We observed in the case of noiseless measurements that H f(x) can be obtained from the measured data for the points $x \in (a, e)$, while f(x) is known for $x \in (b, c)$. The points -1 < a < b < c < e < 1 are specified in figure 4.

Recall the inversion formula for the truncated Hilbert transform:

$$\sqrt{1-x^2}f(x) = C + \frac{1}{\pi}\text{p.v.} \int_{-1}^1 \frac{\text{H}f(y)}{x-y} \sqrt{1-y^2} \, dy$$

and let us split the integral as follows. Define

$$h_1(x) = C + \frac{1}{\pi} \text{p.v.} \int_a^e \frac{Hf(y)}{x - y} \sqrt{1 - y^2} \, dy$$
 (4.1)

$$h_2(x) = \frac{1}{\tau(x)} \frac{1}{\pi} \left[\text{p.v.} \int_{-1}^a \frac{Hf(y)}{x - y} \sqrt{1 - y^2} \, dy + \text{p.v.} \int_e^1 \frac{Hf(y)}{x - y} \sqrt{1 - y^2} \, dy \right], \tag{4.2}$$

where $\tau(x)$ will be specified later and $C = \frac{1}{\pi} \int_{\mathbb{R}} f \, dx = \frac{1}{\pi} \int_{L} \mu \, dl$. That is, we can write

$$\sqrt{1 - x^2} f(x) = h_1(x) + \tau(x)h_2(x), \tag{4.3}$$

where $h_1(x)$ corresponds to the part that could be obtained from noiseless measurements while $h_2(x)$ is defined with the values of $H_1(x)$ that cannot be computed from the measurements. In this context, errors in the measurements translate into errors in the value of $h_1(x)$ and therefore the uniqueness given by corollary 4.1 is lost.

Nonetheless, we would like to know if it is possible to obtain a reasonable reconstruction when the errors in the measurements are small, i.e. when the errors in $R_m(s, \alpha)$ and $g_m(t)$ are small

We will tackle this stability question in two steps. As we mentioned above, $h_1(x)$ corresponds to the part of f(x) that can be obtained from noiseless measurements, and errors in the measurements imply errors in $h_1(x)$. The first step, included in this subsection and the next two, consists in giving a criterion that allows stable reconstruction but which relies on having a bound for the error in $h_1(x)$. The error in $h_1(x)$ is not straightforwardly related to the errors in the measurements $R_m(s,\alpha)$ or the errors in $g_m(t)$, and therefore the criterion presented in this subsection is an indirect one and it is somewhat technical. The second step, which is discussed in subsection 4.5, analyzes how bounds in the errors of $R_m(s,\alpha)$ and $g_m(t)$ can be translated into bounds for the error in $h_1(x)$; i.e. in subsection 4.5, we obtain a set of conditions that directly refer to the errors in $R_m(s,\alpha)$ and $g_m(t)$ and that allow for a stable reconstruction.

Now we focus on the main goal of this subsection: a criterion that ensures that a candidate reconstruction f_r will be close to the original function f, at least for the points inside the interval (a, e). The criterion that leads to the stability bounds of theorems 4.2 and 4.3 is written as $f_r \in S_\epsilon$ (the definition of the set S_ϵ is given below), and it can be roughly summarized as follows. Let Hf_r be the Hilbert transform of the candidate reconstruction f_r and let $h_{1,r}$ be obtained by using equation (4.1) with $Hf_r(y)$ instead of Hf(y) and $C_r := \int_{\mathbb{R}} f_r(y) \, \mathrm{d}y$ instead of $C = \int_{\mathbb{R}} f(y) \, \mathrm{d}y$. We will request that for $x \in (a, e)$ the error of $h_{1,r}(x)$ is not too large, namely we will request that there is a non-negative continuous function E(x) such that

$$|h_{1,r}(x) - h_1(x)| < \epsilon E(x)$$
 for $x \in (a, e)$ with $E(x) \le 1$ for $x \in (b, c)$. (4.4)

This is a somewhat technical condition that amounts to a tight uniform control over the error $|h_{1,r}(x) - h_1(x)|$ in the interval (b, c), while allowing for the possibility of a larger error in the rest of the interval (a, e), as defined by the function E(x). A condition requiring a uniform bound over all of (a, e), especially near a and e, may be too restrictive since, as we approach the region of incomplete measurements, it might be impossible to control the precision of the reconstruction f_r , and $h_{1,r}$ is related to f_r by equation (4.3).

Let us describe explicitly the set S_{ϵ} . Due to the non-local nature of the Hilbert transform, we need to add an *a priori* bound on |Hf| for $x \in (-1, a) \cup (e, 1)$. We know that $f \in C_0^{\infty}(\mathbb{R})$

and therefore $Hf \in C^{\infty}(\mathbb{R})$. Hence, |Hf(x)| is uniformly bounded for $x \in (-1, a) \cup (e, 1)$ and we assume that we know constants M_1 and M_2 such that

$$\frac{1}{\pi}\sqrt{1-x^2}|\mathrm{H}f(x)| \leqslant \begin{cases} M_1/2 & \text{for } x \in (-1,a) \\ M_2/2 & \text{for } x \in (e,1). \end{cases}$$

We define S_{ϵ} as the set of smooth and compactly supported functions $f_r \in C_0^{\infty}(\mathbb{R})$ that satisfy the following four conditions:

(i) supp
$$f_r(x) \subset (-1, 1)$$
 (we know that supp $f(x) \subset (-1, 1)$).

(ii)
$$f_r(x) = f(x)$$
 for $x \in (b, c)$ (recall that $f(x)$ is known in (b, c)).

$$(ii) \ f_r(x) = f(x) \ \text{for} \ x \in (b,c) \ (\text{recall that} \ f(x) \ \text{is known in} \ (b,c)).$$

$$S_\epsilon := \left\{ f_r \in C_0^\infty(\mathbb{R}) : \ (iii) \ |h_{1,r}(x) - h_1(x)| < \epsilon E(x) \ \text{for} \ x \in (a,e) \right\}$$
 with $E(x) \leqslant 1 \ \text{for} \ x \in (b,c)$
$$(iv) \ \frac{1}{\pi} \sqrt{1 - x^2} |Hf_r(x)| < \left\{ \begin{matrix} M_1/2 & \text{for} \ x \in (-1,a) \\ M_2/2 & \text{for} \ x \in (e,1). \end{matrix} \right.$$

The function E(x) is any arbitrary non-negative continuous function on (a, e) satisfying $E(x) \leq 1$ for $x \in (b, c)$.

One of the main results in this paper is to show that for any $f_r \in S_{\epsilon}$, the reconstruction error $|f_r(x) - f(x)|$ is bounded by equation (4.6). Now we make some computations that help us prove such result. Let us denote the reconstruction error as $f_{\rm err}(x) := f_r(x) - f(x)$. Define $h_{1,err}(x)$ and $h_{2,err}(x)$ by using equations (4.1) and (4.2), respectively, with f(x) replaced by $f_{\rm err}(x)$. Observe that equation (4.3) holds with $f_{\rm err}$, $h_{1,\rm err}$ and $h_{2,\rm err}$ instead. The assumption $f_r(x) \in S_{\epsilon}$ translates into

- supp $f_{\text{err}}(x) \subset (-1, 1)$
- $f_{\text{err}}(x) = 0$ for $x \in (b, c)$

$$\begin{aligned} \bullet & |h_{1,\mathrm{err}}(x)| < \epsilon E(x) \text{ for } x \in (a,e) \text{ with } E(x) \leqslant 1 \text{ for } x \in (b,c) \\ \bullet & \frac{1}{\pi} \sqrt{1-x^2} |\mathrm{H} f_{\mathrm{err}}(x)| < \begin{cases} M_1 & \text{for } x \in (-1,a) \\ M_2 & \text{for } x \in (e,1). \end{cases} \end{aligned}$$

We will bound $|f_{err}(x)|$ in terms of ϵ for $x \in (a, b)$. Because of (4.3), it will be enough to bound $\tau(x)h_{2,\text{err}}(x)$ in terms of ϵ for $x \in (a,b)$. The bound we find is not a norm or uniform bound, but instead it is a pointwise bound that depends on the position of x with respect to -1, a, b, c, e, 1.

Since $f_{\text{err}}(x) = 0$ for $x \in (b, c)$, equation (4.3) implies

$$|h_{2,\text{err}}(x)| = \left| \frac{h_{1,\text{err}}(x)}{\tau(x)} \right| < \frac{\epsilon}{|\tau(x)|} \qquad \forall x \in (b,c).$$

$$(4.5)$$

Also, we can extend the definition of $h_{2,err}(z)$ to $z \in \mathcal{C} \setminus ((-1, a) \cup (e, 1))$ by just replacing x by z in the definition of $h_{2,err}(x)$. The extended function $h_{2,err}(z)$ will be analytic in any subset of $\mathcal{C}\setminus((-1,a)\cup(e,1))$ as long as $\tau(z)$ is analytic there. The inclusion of the function $\tau(z)$ in the definition of $h_{2,\mathrm{err}}(z)$ is due to the singular behavior of the integrals $\int_{-1}^{a} \frac{\mathrm{H}f_{\mathrm{err}}(y)}{z-y} \sqrt{1-y^2} \,\mathrm{d}y$ and $\int_{e}^{1} \frac{\mathrm{H}f_{\mathrm{err}}(y)}{z-y} \sqrt{1-y^2} \,\mathrm{d}y$ for $z \in (-1,a)$ and $z \in (e,1)$, respectively. For a fixed domain Ω , we will shortly see that we can choose an analytic function $\tau(z)$ that is easy to analyze and that in Ω has the same behavior as these integrals. In this way, $h_{2,err}(z)$ can be bounded and Nevanlina's principle can be applied.

4.3. Bound for $x \in (a, b)$

Consider Ω to be the disk of diameter (a, c) and remove the subinterval (b, c). Let $D = (b, c) \subset \partial \Omega$ (i.e Ω and D are like in lemma 2.5). Define

$$\tau(z) := \kappa + \int_{-1}^{a} \frac{1}{z - y} \, \mathrm{d}y \qquad \text{with} \qquad \kappa := \frac{M_2 \ln \left(\frac{1 - c}{e - c}\right)}{M_1}.$$

This function $\tau(z)$ is analytic in Ω and, as proved in appendix B, $|h_{2,\text{err}}(z)| < \sqrt{2}M_1$ for $z \in \partial \Omega \backslash D$. Also, for $x \in (b,c)$, $|\tau(x)| = \kappa + \ln\left(\frac{x+1}{x-a}\right)$. Inequality (4.5) then implies $|h_{2,\text{err}}(z)| < \frac{\epsilon}{\kappa + \ln\left(\frac{c+1}{c-a}\right)}$ for $z \in D = (b,c)$. Using Nevanlina's principle (theorem 2.4) and formula (4.3), we conclude the following result.

Theorem 4.2. If f_r is a reconstruction satisfying the conditions imposed by $f_r \in S_{\epsilon}$, where S_{ϵ} is defined in subsection 4.2, then for any $x \in (a, b)$,

$$\sqrt{1-x^2}|f_r(x) - f(x)| < \left[\epsilon E(x) + \sqrt{2}M_1 \left(\kappa + \ln\left(\frac{x+1}{x-a}\right) \right) \left(\frac{\epsilon}{\sqrt{2}M_1 \left(\kappa + \ln\left(\frac{c+1}{c-a}\right) \right)} \right)^{1-\omega(x)} \right]. \tag{4.6}$$

The function $\omega(x) = \frac{4}{\pi} \arctan \sqrt{\frac{2(b-x)(c-a)}{(c-a)^2-(2b-a-c)(2x-a-c)}}$ is Nevanlina's exponent that was calculated in lemma 2.5.

In order to identify the consequence of this result, we rewrite the bound in theorem 4.2 in a less explicit form (assume $0 < \epsilon \le 1$):

$$|f_r(x) - f(x)| \le K(x)\epsilon^{\delta(x)}$$
, with $\delta(x) = 1 - \omega(x)$.

The function $\delta(x) > 0$ is continuous and satisfies $\lim_{x \to b} \delta(x) = 1$ and $\lim_{x \to a} \delta(x) = 0$. The function K(x) is also continuous and $\lim_{x \to b} K(x) = \left(\kappa + \ln\left(\frac{b+1}{b-a}\right)\right) / \left(\kappa + \ln\left(\frac{c+1}{c-a}\right)\right) < \infty$ while $\lim_{x \to a} K(x) = \infty$. Written in this form, it is easier to see that the bound (4.6) implies the following: an accurate reconstruction is possible near b and the reconstruction should become more unstable as we approach a.

With respect to the reconstruction of μ over the line L, theorem 4.2 implies that the reconstruction should be accurate near region A, where μ is assumed to be known, while the reconstruction should be less accurate as we move far from region A toward the region of incomplete measurements.

By symmetry, the points in the interval (c, e) admit a bound of exactly the same kind. We skip such computation and move on to study the case of a different region A.

4.4. Points between regions where μ is known

We study what happens when we restrict the attenuation function μ to a line L as that in figure 5(a). As before, we reduce the analysis to a 1D problem, and uniqueness follows in the same way.

We modify the list of conditions that imply a bound for the reconstruction error, according to the situation presented in figure 5. Let us define \tilde{S}_{ϵ} as the set of smooth compactly supported

function f_r satisfying

$$(i) \ \operatorname{supp} f_r(x) \subset (-1,1) \\ (ii) \ f_r(x) = f(x) \ \operatorname{for} \ x \in (b,c) \cup (d,e) \\ \tilde{S}_{\epsilon} := \begin{cases} (iii) \ |h_{1,r}(x) - h_1(x)| < \epsilon E(x) \ \operatorname{for} \ x \in (a,e) \\ f_r \in C_0^{\infty}(\mathbb{R}) : & \text{with } E(x) \leqslant 1 \ \operatorname{for} \ x \in (b,c) \cup (d,e) \end{cases} .$$

$$(iv) \ \frac{1}{\pi} \sqrt{1 - x^2} |\operatorname{H} f_r(x)| < \begin{cases} M_1/2 & \text{for } x \in (-1,a) \\ M_2/2 & \text{for } x \in (e,1). \end{cases}$$

As in subsection 4.2, let $f_{err}(x) := f_r(x) - f(x)$ denote the reconstruction error. Since $f_r \in \tilde{S}_{\epsilon}$, the following set of conditions replace those of subsection 4.2:

- supp $f_{\text{err}}(x) \subset (-1, 1)$
- $f_{\text{err}}(x) = 0$ for $x \in (b, c) \cup (d, e)$

•
$$|h_{1,\text{err}}(x)| < \epsilon E(x) \text{ for } x \in (a, e) \text{ with } E(x) \le 1 \text{ for } x \in (b, c) \cup (d, e).$$

• $\frac{1}{\pi} \sqrt{1 - x^2} |H_{ferr}(x)| < \begin{cases} M_1 & \text{for } x \in (-1, a) \\ M_2 & \text{for } x \in (e, 1) \end{cases}$

To obtain a bound for the reconstruction error, it is enough to bound $h_{2,err}(x)$. In order to do this, we consider adequate domains Ω = {a disk minus a subinterval of the diameter} and functions $\tau(z)$ with the right behavior in each Ω . Applications of Nevanlina's principle for $h_{2,err}(z)$ will then produce the desired bounds.

The interval (c, d) is contained in the domains Ω_1 and Ω_2 described in figure 5(b). Namely, we obtain Ω_1 by removing the interval $D_1 = (b, c)$ from the disk of diameter (b, d). Since Ω_1 is far from $(-1, a) \cup (e, 1)$, we can consider different candidates for the function $\tau(z)$. We obtain Ω_2 by removing the interval $D_2 = (d, e)$ from the disk of diameter (c, e). Let us define the following functions:

$$\tau_1(z) := \kappa_1 + \int_{-1}^a \frac{1}{z - y} \, \mathrm{d}y \qquad \text{with} \qquad \kappa_1 := \frac{M_2 \ln\left(\frac{1 - d}{e - d}\right)}{M_1}$$

$$\tau_2(z) := \kappa_2 + \int_e^1 \frac{1}{y - z} \, \mathrm{d}y \qquad \text{with} \qquad \kappa_2 := \frac{M_1 \ln\left(\frac{c + 1}{c - a}\right)}{M_2}$$

$$\tau_3(z) := \kappa_3 + \int_e^1 \frac{1}{y - z} \, \mathrm{d}y \qquad \text{with} \qquad \kappa_3 := \frac{M_1 \ln\left(\frac{b + 1}{b - a}\right)}{M_2}.$$

After a slight modification of appendix B, the analysis leading to theorem 4.2 is valid for Ω_1 with $\tau_1(z)$, for Ω_2 with $\tau_2(z)$ and for Ω_1 with $\tau_3(z)$. The application of Nevanlina's principle on these three different settings provides us with the bounds (4.7)–(4.9) respectively in theorem 4.3. In addition to that, since Ω_1 is far from $(-1, a) \cup (e, 1)$ then $h_{2,err}(z)$ does not have a singular behavior in Ω_1 , and we can consider Ω_1 with $\tau_4(z) := 1$. Inequality (4.5) implies $|h_{2,\text{err}}(z)| \le \epsilon$ for $z \in (b,c)$, while the second part of appendix B shows that $|h_{2,\text{err}}(z)| \le M_1 \ln\left(\frac{c+1}{c-a}\right) + M_2 \ln\left(\frac{1-d}{e-d}\right)$ for $z \in \partial \Omega_1 \backslash D_1$. An application of Nevanlina's principle in this case provides us with the bound (4.10) in theorem 4.3.

Theorem 4.3. For a reconstruction $f_r(x)$ satisfying $f_r \in \tilde{S}_{\epsilon}$, we have the following bounds at points $x \in (c, d)$. Using Ω_1 with $\tau_1(z)$, we obtain

$$\sqrt{1 - x^{2}} | f_{r}(x) - f(x) |
< \left[\epsilon E(x) + \sqrt{2} M_{1} \left(\kappa_{1} + \ln \left(\frac{x+1}{x-a} \right) \right) \left(\frac{\epsilon}{\sqrt{2} M_{1} \left(\kappa_{1} + \ln \left(\frac{c+1}{c-a} \right) \right)} \right)^{1 - \omega_{1}(x)} \right], \quad (4.7)$$

$$where \omega_{1}(x) = \frac{4}{\pi} \arctan \sqrt{\frac{2(x-c)(d-b)}{(d-b)^{2} - (2c-d-b)(2x-d-b)}}.$$

Using Ω_2 with $\tau_2(z)$, we obtain

$$\sqrt{1-x^2}|f_r(x)-f(x)| < \left[\epsilon E(x) + \sqrt{2}M_2\left(\kappa_2 + \ln\left(\frac{1-x}{e-x}\right)\right) \left(\frac{\epsilon}{\sqrt{2}M_2(\kappa_2 + \ln\left(\frac{1-d}{e}\right))}\right)^{1-\omega_2(x)}\right], \quad (4.8)$$

where $\omega_2(x) = \frac{4}{\pi} \arctan \sqrt{\frac{2(d-x)(e-c)}{(e-c)^2 - (2d-c-e)(2x-c-e)}}$.

Using Ω_1 with $\tau_3(z)$, we obtain

$$\sqrt{1-x^2}|f_r(x)-f(x)| < \left[\epsilon E(x) + \sqrt{2}M_2\left(\kappa_3 + \ln\left(\frac{1-x}{e-x}\right)\right) \left(\frac{\epsilon}{\sqrt{2}M_3\left(\kappa_2 + \ln\left(\frac{1-d}{e}\right)\right)}\right)^{1-\omega_1(x)}\right]. \tag{4.9}$$

Using Ω_1 with $\tau_4(z) := 1$, we obtain

$$\sqrt{1-x^2}|f_r(x) - f(x)| < \left[\epsilon E(x) + \left(M_1 \ln\left(\frac{b+1}{b-a}\right)\right) + M_2 \ln\left(\frac{1-d}{e-d}\right)\right) \left(\frac{\epsilon}{M_1 \ln\left(\frac{b+1}{b-a}\right) + M_2 \ln\left(\frac{1-d}{e-d}\right)}\right)^{1-\omega_1(x)}\right].$$
(4.10)

Which bound is better actually depends on the values of a, b, c, d, e, M_1, M_2 and the location of the point x in the interval (c, d).

Let us rewrite the combination of the bounds in theorem 4.3 in a less explicit way (assume $\epsilon \leq 1$):

$$|f_r(x) - f(x)| \le K(x)\epsilon^{\delta(x)}$$

with $\delta(x) > 0$ and K(x) being continuous. The main difference with respect to the bound in subsection 4.3 is that now, by putting together the bounds in theorem 4.3, the functions $\delta(x)$ and K(x) satisfy $\lim_{x\to c} \delta(x) = \lim_{x\to d} \delta(x) = 1$, while $\lim_{x\to c} K(x) < \infty$ and $\lim_{x\to d} K(x) < \infty$. In particular, for $\delta = \min_{(c,d)} \delta(x) > 0$ and $K = \max_{(c,d)} K(x) < \infty$, we have

$$|f_r(x) - f(x)| \le K\epsilon^{\delta}$$
.

This is a uniform bound for the reconstruction of f in the interval (c, d). The intuition that stability should be achievable inside the whole interval (c, d) is verified: when we move inside the interval (c, d), we stay away from the regions of incomplete data.

4.5. Stability based on measurement errors

In the previous subsections, we bounded the reconstruction error $|f_r(x) - f(x)|$ for the points x inside the FOV. But these results are not easy to interpret because they require $f_r \in S_{\epsilon}$, and this means that we have to bound the error $|h_{1,r}(x) - h_1(x)|$ of the intermediate function $h_1(x)$ defined by equation (4.1). A more useful error bound for the reconstruction would be expressed in terms of the error for quantities related directly to the measurements, namely $R_m(s,\alpha)$ and $g_m(t)$.

In this subsection, we study how to bound the reconstruction error only from the knowledge that $R_m(s, \alpha)$ and $g_m(t)$ contain small errors plus the *a priori* knowledge. The answer is not straightforward. The condition $f_r \in S_{\epsilon}$ requires us to bound $|h_{1,r}(x) - h_1(x)|$, and $h_1(x)$ is computed from $H_f(x)$ as defined in equation (4.1). In the noiseless case we know that $g_m(x) = H_f(x)$ and therefore, even in the presence of noise, we may want to construct f_r

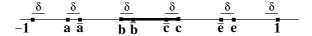


Figure 6. Relevant intervals after smoothing.

such that $Hf_r = g_m$; this is a good idea but it does not produce $f_r \in S_{\epsilon}$: even if the error $|Hf_r - Hf|$ is very small, there is no guarantee that $h_{1,r}$ will be close to h_1 (such a fact can be noted by observing that the Hilbert transform of a discontinuous function is not bounded, and it would be unrealistic to assume continuity constraints on the error $|g_m - Hf|$).

We overcome this problem by reconstructing instead a smooth approximation \overline{f} of the original attenuation function f. We define $\overline{f}(x) := \phi * f(x) := \int_{\mathbb{R}} \phi(x-y) f(y) \, \mathrm{d}y$ as the convolution of f with a smooth non-negative blurring kernel $\phi(x) \in C_0^\infty(\mathbb{R})$, ϕ being such that $\int_{\mathbb{R}} \phi(x) \, \mathrm{d}x = 1$ and with bounded support supp $\phi \subset (-\delta, \delta)$. We will consider the situation studied in subsection 4.2 (see figure 4) and we assume that $\delta > 0$ is small enough to satisfy $-1 + \delta < a, b + \delta < c - \delta, e < 1 - \delta$ (see figure 6).

We assume the following a priori information about f:

- supp $f \subset (-1 + \delta, 1 \delta)$; hence supp $\overline{f} \subset (-1, 1)$.
- f(x) is known for $x \in (b, c)$.
- We know constants M_1 and M_2 such that

$$\frac{1}{\pi}|Hf(x)| \leqslant \begin{cases} M_1/2 & \text{for } x \in (-1-\delta, a+2\delta) \\ M_2/2 & \text{for } x \in (e-2\delta, 1+\delta). \end{cases}$$

We also assume that the error in the measurements is small, as prescribed by the following bounds:

$$|g_m(x) - Hf(x)| < \epsilon$$
 for $x \in (a, e)$ and $|R_m \mu(s_0, \alpha_0) - R\mu(s_0, \alpha_0)| < \epsilon$,
$$(4.11)$$

where (s_0, α_0) parameterize the line L that defines f; hence $R\mu(s_0, \alpha_0) = \int_{\mathbb{R}} f(y) \, dy$. We define the set A_{ϵ} of *admissible* solution estimates as

(i) supp $f_r \subset (-1 + \delta, 1 - \delta)$

$$(ii) \ f_r(x) = f(x) \text{ for } x \in (b, c)$$

$$A_{\epsilon} := \begin{cases} f_r \in C_0^{\infty}(\mathbb{R}) : (iii) \frac{1}{\pi} |Hf_r(x)| \leq \begin{cases} M_1/2 & \text{for } x \in (-1 - \delta, a + 2\delta) \\ M_2/2 & \text{for } x \in (e - 2\delta, 1 + \delta) \end{cases}$$

$$(iv) \ Hf_r(x) - g_m(x) = \lambda(x) \text{ for some } \lambda \text{ with } |\lambda(x)| < \epsilon \text{ for } x \in (a, e)$$

$$(v) \ \left| \int_{\mathbb{R}} f_r(y) \, \mathrm{d}y - R_m \mu(s_0, \alpha_0) \right| < \epsilon.$$

The first three conditions in the definition of A_{ϵ} correspond exactly to the *a priori* knowledge about f(x). The last two conditions in A_{ϵ} correspond to the bounds of the measurement errors, as specified by (4.11). Therefore the original function f(x) is an admissible solution, i.e. $f \in A_{\epsilon}$, and if $f_r \in A_{\epsilon}$ we will say that f_r is compatible with the *a priori* information and the measurements.

As mentioned before, just the fact that $f_r \in A_{\epsilon}$ does not guarantee that $f_r \in S_{\epsilon}$. However, what we will show is that for any admissible solution $f_r \in A_{\epsilon}$ the convolution $\phi * f_r(x)$, as a reconstruction of $\overline{f}(x) = \phi * f(x)$, has a bounded reconstruction error. In order to establish

that let us define $\overline{a}=a+\delta, \overline{b}=b+\delta, \overline{c}=c-\delta$ and $\overline{e}=e-\delta$ (see figure 6) and let us define the set

$$(i) \operatorname{supp} \overline{f}_r \subset (-1, 1)$$

$$(ii) \overline{f}_r(x) = \overline{f}(x) \text{ for } x \in (\overline{b}, \overline{c})$$

$$\overline{A_{\epsilon}} := \begin{cases} \overline{f}_r \in C_0^{\infty}(\mathbb{R}) : (iii) \frac{1}{\pi} \sqrt{1 - x^2} | H \overline{f}_r(x) | \leq \begin{cases} M_1/2 & \text{for } x \in (-1, \overline{a}) \\ M_2/2 & \text{for } x \in (\overline{e}, 1) \end{cases}$$

$$(iv) H \overline{f}_r(x) - \phi * g_m(x) = \phi * \lambda(x) \text{ for some } |\lambda(x)| < \epsilon \text{ for } x \in (a, e)$$

$$(v) \left| \int_{\mathbb{R}} \overline{f}_r(y) \, \mathrm{d}y - R_m \mu(s_0, \alpha_0) \right| < \epsilon.$$

Since $\phi*(\mathrm{H}f)=\mathrm{H}(\phi*f)$, it is easy to check that if $f_r\in A_\epsilon$ then $\phi*f_r\in\overline{A_\epsilon}$. In particular, $\overline{f}\in\overline{A_\epsilon}$. We also define the following set:

$$(i) \operatorname{supp} \overline{f}_r(x) \subset (-1, 1)$$

$$(ii) \overline{f}_r(x) = \overline{f}(x) \text{ for } x \in (\overline{b}, \overline{c})$$

$$\overline{S}_{\overline{\epsilon}} := \left\{ \overline{f}_r \in C_0^{\infty}(\mathbb{R}) : (iii) \frac{1}{\pi} \sqrt{1 - x^2} |H\overline{f}_r(x)| < \begin{cases} M_1/2 & \text{for } x \in (-1, \overline{a}) \\ M_2/2 & \text{for } x \in (\overline{e}, 1) \end{cases} \right\}$$

$$(iv) |\overline{h}_{1,r}(x) - \overline{h}_1(x)| < \overline{\epsilon} \overline{E}(x) \text{ for } x \in (\overline{a}, \overline{e})$$

$$\text{with } \overline{E}(x) \leqslant 1 \text{ for } x \in (\overline{b}, \overline{c}),$$

where $\overline{h}_{1,r}(x)$ (respectively $\overline{h}_1(x)$) are calculated using equation (4.1) with \overline{f}_r instead of f (respectively \overline{f} instead of f), and with \overline{a} and \overline{e} instead of a and e. The constant $\overline{\epsilon}$ is proportional to ϵ and $\overline{E}(x)$ is a continuous function in $(\overline{a},\overline{e})$ with $\overline{E}(x) \leq 1$ for $x \in (\overline{b},\overline{c})$. The precise description of \overline{e} and $\overline{E}(x)$ is given in appendix C, where it is also shown that if (4.11) holds then $\overline{A_{\epsilon}} \subset \overline{S_{\overline{\epsilon}}}$ and therefore $\phi * f_r \in \overline{S_{\overline{\epsilon}}}$ for any $f_r \in A_{\epsilon}$. Let us stop for a moment to note the following: the last two conditions in the definition of $\overline{A_{\epsilon}}$ are bounds of the candidates compared to the measurements, but the last condition in $\overline{S_{\overline{\epsilon}}}$ involves \overline{f} and not the measurements. Roughly speaking, this transition is possible because $\overline{f} \in \overline{A_{\epsilon}}$ and all the functions in $\overline{A_{\epsilon}}$ are close to each other.

We observe that the set $\overline{S}_{\overline{\epsilon}}$ coincides with the criterion introduced in subsection 4.2 (listed in the set S_{ϵ}), provided that we replace a, b, c, e, ϵ and E(x) by $\overline{a}, \overline{b}, \overline{c}, \overline{e}, \overline{\epsilon}$ and $\overline{E}(x)$. Using theorem 4.2, we conclude that for any admissible solution $f_r \in A_{\epsilon}$ the error $|\phi * f_r(x) - \overline{f}(x)|$ will be bounded by equation (4.6), with the corresponding substitutions.

5. Numerical experiments

In order to support numerically the previous results, we consider the situation described in figure 7(a). The Shepp–Logan phantom is enlarged 2.5 times, so its ellipse axes are 4.6 and 3.45. We consider a rectangular FOV of 1.5×2 located in the center of the phantom; the fact that the FOV is a rectangle does not change the theory and makes the presentation of the numerical results clearer. A total of 1200 parallel-beam projections over an angular range of 180° are computed. On each projection, lines are sampled at every 2/256 of distance and the lines not intersecting the FOV are truncated. The FOV is reconstructed as an image of 192×256 pixels.

The gray strips in figure 7(b) correspond to region A, where the attenuation is known a priori. Region A divides the FOV into regions B, C and D to the left, in between and to the right of A respectively. With respect to the support of the object, we consider two situations (see figure 7(c)): we have the knowledge that the phantom is contained inside a region 1.2

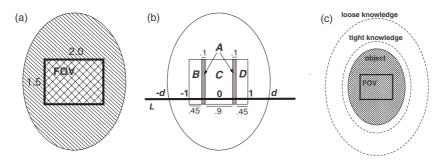


Figure 7. Description of the numerical experiment. (a) The rectangular FOV is completely contained in the Shepp–Logan phantom. (b) The attenuation μ is known in region A. We use DBP on horizontal lines L. (c) We assume that we approximately know the support of the object.

times its original size, labeled a 'tight support' case, or we have the knowledge that the object is contained in a region 1.8 times its original size, labeled a 'loose support' case.

Consider a horizontal line L as the one in figure 7(b). Let f(x) be the restriction of μ to that line and let $f_r(x)$ be the reconstruction of f(x). The *a priori* knowledge on μ corresponds to the following knowledge on f(x):

- (i) f(x) is known $\forall x \in (-0.55, -0.45) \cup (0.45, 0.55)$.
- (ii) $f(x) = 0 \ \forall x \notin (-d_i, d_i)$. Let d be the intersection of the line L and the boundary of the phantom as in figure 7, $d_i = 1.2 \times d$ for the 'tight support' case, $d_i = 1.8 \times d$ for the 'loose support' case.
- (iii) $f(x) \ge 0$ since it is a density function.

From the measurements, we compute

- (i) $g_m(x) \ \forall x \in (-1, 1)$, computed using the measurements in the DBP formula (3.2).
- (ii) $R_m \mu(s, \frac{\pi}{2})$, the measurement on the horizontal line L.

The reconstruction of f(x) is done by trying to find a function f_r in the intersection of the following sets:

```
E_{1} := \{ \tilde{f} \in L^{2}(\mathbb{R}) : \tilde{f}(x) = f(x) \, \forall \, x \in (-.55, -.45) \cup (.45, .55) \}
E_{2} := \{ \tilde{f} \in L^{2}(\mathbb{R}) : \tilde{f}(x) = 0 \, \forall \, x \notin (-d_{i}, d_{i}) \}
E_{3} := \{ \tilde{f} \in L^{2}(\mathbb{R}) : \tilde{f}(x) \geq 0 \}
E_{4} := \{ \tilde{f} \in L^{2}(\mathbb{R}) : |H\tilde{f}(x) - g_{m}(x)| \leq \epsilon \, \forall \, x \in (-1, 1) \}
E_{5} := \{ \tilde{f} \in L^{2}(\mathbb{R}) : \int_{-d_{i}}^{d_{i}} \tilde{f}(x) \, dx = R_{m} \mu \left( s, \frac{\pi}{2} \right) \right\}.
```

Observing that the mentioned sets are convex, the scheme followed to find $f_r(x)$ in the intersection of E_i is by iteratively projecting into them, in the order E_2 , E_4 , E_1 , E_5 , E_3 . The projection operators on the sets above are straightforward except for the projection on E_4 . Denote as $P_4: L^2 \to E_4 \subset L^2$ the orthogonal projection on E_4 . This operator takes the following form [11]: for $\tilde{f} \in L^2(\mathbb{R})$ let

$$\varphi(x) := \begin{cases} H\tilde{f}(x) & x \notin (-1,1) \\ \max\{g_m(x) - \epsilon, \min\{g_m(x) + \epsilon, H\tilde{f}(x)\}\} & x \in (-1,1) \end{cases}$$

then $P_4\tilde{f} = \mathrm{H}^{-1}\varphi$.

The methodology described above is essentially the DBP-POCS method in [11].

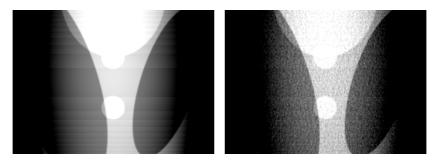


Figure 8. Left: noiseless reconstruction with only the 'tight support' knowledge. The display window is [0.874,0.926] instead of [0.994,1.046]. Right: reconstruction with noise and 'tight support' knowledge, display window [0.874,0.926].

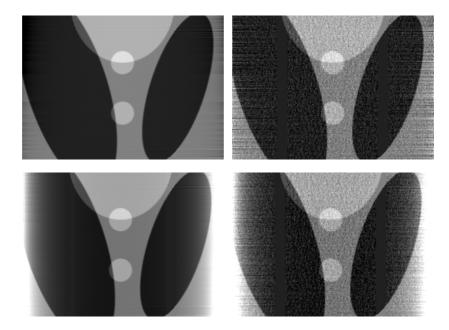


Figure 9. Top left: noiseless reconstruction with *a priori* knowledge in *A* and 'tight support' knowledge. Top right: reconstruction under noise with knowledge as in top left. Bottom left: noiseless reconstruction with *a priori* knowledge in *A* and 'loose support' knowledge. Bottom right: reconstruction under noise with knowledge as in bottom left. All reconstructions displayed on the original phantom display window [0.994,1.046].

In figure 8 we present the reconstruction obtained if we do not include the *a priori* knowledge, i.e. without projecting on E_1 . Without the *a priori* knowledge, the reconstructed value of the attenuation function is shifted and it presents strong low frequency artifacts; this is a large bias in the reconstruction and is the kind of behavior that usually shows up in the interior problem. Reconstructions including the *a priori* knowledge, i.e. including the projection on E_1 , are shown in figure 9. For region C, contained in between regions of *a priori* knowledge, we observe that reconstructions are accurate and stable even with noisy data and only with loose knowledge about the support of the attenuation. In regions B and D, the reconstructions tend to be more accurate near the region of *a priori* knowledge and become less accurate as we move away from it. Artifacts appear toward the region of incomplete measurements

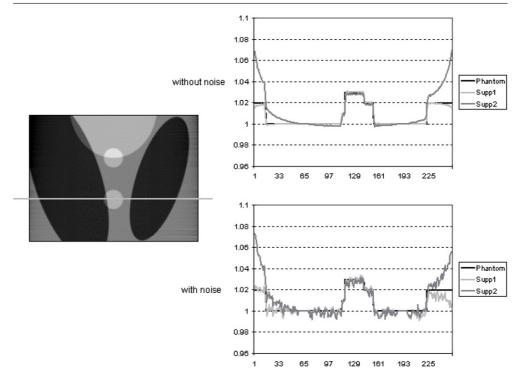


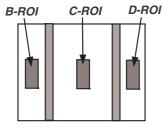
Figure 10. Example of a profile line of the reconstruction, supp1 and supp2 correspond to the 'tight support' and 'loose support' cases respectively. The first graph is noiseless reconstruction, the second graph is the profile of noisy reconstruction. With no noise added to the data, the reconstruction with support 1 is very close to the original phantom, except near the edges; accordingly, the curves for these two images can only be distinguished near the edges.

and reconstruction near the region of incomplete measurements depends particularly on the knowledge about the support of the function. The quantitative aspects of the reconstructions in figure 9 are also illustrated by profiles in figure 10.

The table in figure 11 shows the effect of noisy data for reconstruction, with and without *a priori* knowledge, in the 'tight support' case. We also include the bias of the reconstruction with respect to the original phantom. Namely, let $\mu(x)$ be the attenuation function of the original phantom, $\mu_r(x)$ be the reconstruction without noise and $\mu_{r,n}(x)$ be the reconstruction obtained with Poisson noise added to the data. On each ROI, we compute the standard deviations and biases as

$$\mathrm{SD}_{\mathrm{ROI}} = \sqrt{\frac{\sum_{x \in \mathrm{ROI}} (\mu_r(x) - \mu_{r,n}(x))^2}{\#\{x : x \in \mathrm{ROI}\}}}, \qquad \quad \mathrm{BIAS}_{\mathrm{ROI}} = \frac{\sum_{x \in \mathrm{ROI}} |\mu(x) - \mu_r(x)|}{\#\{x : x \in \mathrm{ROI}\}}.$$

We notice in figure 11 that all the standard deviations, with and without *a priori* knowledge, are on the same order of magnitude, while the bias in the reconstruction with *a priori* knowledge is much smaller than the bias in the reconstruction without *a priori* knowledge. We also observe that, going from reconstruction without *a priori* knowledge to reconstruction with *a priori* knowledge, the standard deviation in regions *B* and *D* increases by 12% and 15% respectively, while in region *C* the standard deviation increases only by 1.6% (and becomes about 3% smaller than the standard deviations in regions *B* and *D*). That is, for the ROI *C*, located between regions of *a priori* knowledge, the reconstruction that includes the *a priori*



	SD and Bias.	SD and Bias. "Tight
	Only "Tight support"	support" + μ known in A
B-ROI	2.89×10^{-3} 0.15	$3.32 \times 10^{-3} \mid 2.09 \times 10^{-04}$
C-ROI	3.16×10^{-3} 0.10	$3.21 \times 10^{-3} \mid 3.74 \times 10^{-04}$
D-ROI	2.95×10^{-3} 0.15	3.30×10^{-3} 3.58×10^{-04}

Figure 11. SD shows the standard deviation of the noisy reconstruction with respect to the noiseless reconstruction. Bias shows the average bias of the noiseless reconstruction compared to the original phantom. The size of each ROI is 0.4×0.2 .

knowledge is much more accurate than the reconstruction without the *a priori* knowledge while the standard deviation remains essentially unchanged.

6. Extensions

For theorems 4.2 and 4.3, we can relax our *a priori* knowledge on the attenuation function. For the *a priori* knowledge, it is enough to assume that we know $\mu_{\epsilon_0}(x)$ such that $|\mu_{\epsilon_0}(x) - \mu(x)| \le \epsilon_0$ for $x \in A$. In the computations leading to theorems 4.2 and 4.3, this extra ϵ_0 can be absorbed in $h_{1,\text{err}}$, and the bounds presented in theorems 4.2 and 4.3 are still valid if we replace ϵ by $\epsilon + \epsilon_0$.

A second extension is with respect to the acquisition geometry assumed in this paper. We assumed that the measurements were either acquired in parallel-beam geometry or that they were rebinned into a parallel-beam parametrization. This assumption was done in order to simplify the presentation, and it is not strictly necessary. The explicit parallel-beam parametrization was used only in corollary 3.2. There is an analogous formula relating the fan-beam or cone-beam measurements to the directional Hilbert transform [24]. Once the directional Hilbert transform of the attenuation function is obtained, the rest of the analysis is the same. An extension to the fan-beam geometry is direct. Nonetheless, in the case of cone-beam geometry, truncation of the data set can take a complicated form, and it is not easy to characterize all the segments along which the directional Hilbert transform can be computed from the available data.

Throughout the paper, we have been picturing the FOV as a circular region. However, as we saw with the simulation, the FOV does not need to be circular; it can be rectangular or it can take less regular shapes. Note, however, that the FOV will always be convex or the union of disjoint convex sets [3].

7. Conclusion

In the present paper, we studied the interior problem of computerized tomography. We concluded that adding extra knowledge to the support of the attenuation function, and adding knowledge of the value of the attenuation function in a subregion of the FOV, the measurements are enough to uniquely determine the function all over the object. Additionally, we proved that any candidate reconstruction satisfying the set of conditions in subsection 4.2 (or the conditions in subsection 4.4) has a reconstruction error bounded by equation (4.6) (respectively equations (4.7)–(4.10)). These bounds establish that accurate reconstruction is possible for

points inside the FOV if they are near the region where the attenuation is known. The same bounds suggest that reconstruction becomes unavoidably unstable as we approach the region of incomplete measurements. Last, we showed that reconstruction can be stable along any interval in the FOV that is contained in between two regions where the attenuation is known. All our theoretical predictions were illustrated by numerical reconstructions using the DBP-POCS method of [11]. The reconstructed attenuation showed good accuracy and stability as suggested by theorems 4.2 and 4.3, thus supporting our results for the interior problem with *a priori* knowledge.

The possibility of stable reconstruction for the interior problem has interesting consequences for the problem of computed tomography with truncated data. For example, in low-dose cardiac CT the region of interest is well inside the patient and image reconstruction on a reduced FOV translates into a reduced radiation dose. The required *a priori* knowledge about the support of the attenuation function is easy to obtain, at least loosely (the patient is inside the scanner). It is more difficult to obtain the *a priori* knowledge of the attenuation function in a subregion of the FOV. Some suggestions are to complement the CT measurements with other imaging techniques or to try to identify a region of tissue or bone inside the FOV for which the attenuation function can be guessed with good enough accuracy.

A case in which *a priori* knowledge is not hard to obtain is when performing multiple CT scans of the same region in a short period of time, for instance when conducting a scan before and after a contrast agent has been administered. With the first full scan the non-dyed attenuation coefficients are determined, and any region not affected by the contrast agent is a region of *a priori* knowledge for the subsequent scans. If such a region can be identified and we are interested only in an image of a localized region well inside the body (as in the case of urography), the results of stable reconstruction for the interior problem with *a priori* knowledge would allow us to reduce the FOV for the subsequent scans and therefore reduce the overall radiation dose on the patient.

Acknowledgments

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Appendix A

We say that a function f is in $C^{\sigma}(\mathbb{R}^n)$, with $0 < \sigma \leq 1$, if for any point $x \in \mathbb{R}^n$ there exist constants C and $\delta > 0$ such that

$$|f(y) - f(x)| < C|x - y|^{\sigma}$$
 for any y satisfying $|y - x| < \delta$.

We say $f \in C^{\infty}(\mathbb{R})$ if it is differentiable to any order.

The support of a function f, denoted as supp f, is defined as the complement of the largest open set where f vanishes. We say that $f \in C_0^{\sigma}(\mathbb{R}^n)$ if it is in $C^{\sigma}(\mathbb{R}^n)$ and also has compact support. Analogously for $C_0^{\infty}(\mathbb{R}^n)$.

Appendix B

Let Ω be the disc of diameter (a, c) with -1 < a < c < e < 1 and let

$$k(z) := \frac{1}{\pi} \left[\text{p.v.} \int_{-1}^{a} \frac{Hf(t)}{z - t} \sqrt{1 - t^2} \, dt + \text{p.v.} \int_{e}^{1} \frac{Hf(t)}{z - t} \sqrt{1 - t^2} \, dt \right].$$

Assume that

$$\frac{1}{\pi}\sqrt{1-t^2}|Hf(t)| < \begin{cases} M_1 & \text{for } t \in (-1,a) \\ M_2 & \text{for } t \in (e,1) \end{cases};$$

then for z = x + iy with $Re(z) = x \in (a, c)$, we have

$$\begin{split} |k(z)| &< M_1 \left| \int_{-1}^a \frac{1}{z - t} \, \mathrm{d}t \right| + M_2 \int_e^1 \left| \frac{1}{t - z} \right| \mathrm{d}t \\ &\leqslant M_1 \left| \int_{-1}^a \frac{1}{z - t} \, \mathrm{d}t \right| + M_2 \int_e^1 \frac{1}{t - x} \, \mathrm{d}t \\ &\leqslant M_1 \left(\left| \int_{-1}^a \frac{1}{z - t} \, \mathrm{d}t \right| + \frac{M_2 \ln \left(\frac{1 - c}{e - c} \right)}{M_1} \right) \\ &\leqslant \sqrt{2} M_1 \left| \int_{-1}^a \frac{1}{z - t} \, \mathrm{d}t + \frac{M_2 \ln \left(\frac{1 - c}{e - c} \right)}{M_1} \right|, \end{split}$$

where the last step is valid since $\operatorname{Re}\left(\int_{-1}^{a}\frac{1}{z-t}\,dt\right)$ and $\frac{M_{2}\ln\left(\frac{1-c}{e-c}\right)}{M_{1}}$ are both non-negative. Additionally, for $z=x+\mathrm{i}y$ with $\operatorname{Re}(z)=x\in(c,d)$ we also have

$$|k(z)| < M_1 \left| \int_{-1}^a \frac{1}{z - t} dt \right| + M_2 \int_e^1 \left| \frac{1}{t - z} \right| dt$$

$$\leq M_1 \int_{-1}^a \frac{1}{x - t} dt + M_2 \int_e^1 \frac{1}{t - x} dt$$

$$\leq M_1 \ln \left(\frac{b + 1}{b - a} \right) + M_2 \ln \left(\frac{1 - d}{e - d} \right).$$

Appendix C

As mentioned in subsection 4.5, assuming that (4.11) holds, we want to prove that $\overline{A_{\epsilon}} \subset \overline{S_{\epsilon}}$. The constant $\overline{\epsilon}$ will be proportional to ϵ and $\overline{E}(x)$ will be a continuous function in $(\overline{a}, \overline{e})$ with $\overline{E}(x) \leqslant 1$ for $x \in (\overline{b}, \overline{c})$. Recall that $\phi \in C_0^{\infty}(\mathbb{R})$ is such that $\int_{\mathbb{R}} \phi(x) \, \mathrm{d}x = 1$ and $\sup \phi \subset (-\delta, \delta)$.

We assume that (4.11) holds, i.e. we assume that

$$|g_m(x) - Hf(x)| < \epsilon \text{ for } x \in (a, e) \text{ and } |R_m \mu(s_0, \alpha_0) - R\mu(s_0, \alpha_0)| < \epsilon, \tag{C.1}$$

and given (C.1) we want to prove that the following two conditions:

$$H\overline{f}_r(x) - \phi * g_m(x) = \phi * \lambda(x) \text{ for } x \in (\overline{a}, \overline{e}) \text{ for some } |\lambda(x)| < \epsilon \text{ for } x \in (a, e)$$
 (C.2)

$$\left| \int_{\mathbb{R}} \overline{f}_r(y) \, \mathrm{d}y - R_m \mu(s_0, \alpha_0) \right| \leqslant \epsilon \tag{C.3}$$

imply

$$|\overline{h}_{1,r}(x) - \overline{h}_1(x)| < \overline{\epsilon}\overline{E}(x) \text{ for } x \in (\overline{a}, \overline{e}) \text{ with } \overline{E}(x) \le 1 \text{ for } x \in (\overline{b}, \overline{c}), (C.4)$$

where $\overline{h}_{1,r}(x)$ (respectively $\overline{h}_1(x)$) are calculated using equation (4.1) with \overline{f}_r instead of f (respectively $\overline{f} := \phi * f$ instead of f), and with $\overline{a} := a + \delta$ and $\overline{e} := e - \delta$ instead of a and e.

First, we will use (C.1) to eliminate reference to the measurements in (C.2) and (C.3). Recall that $\phi * (Hf) = H(\phi * f) = H\overline{f}$ and that the convolution is linear. Hence, (C.2) implies

$$H\overline{f}_r(x) - H\overline{f}(x) = [H\overline{f}_r(x) - \phi * g_m(x)] + [\phi * g_m(x) - \phi * Hf(x)]$$
$$= \phi * (\lambda(x) + [g_m(x) - Hf(x)]),$$

and letting $\tilde{\lambda}(x) := \lambda(x) + [g_m(x) - Hf(x)]$ the first bound in (C.1) allows us to replace (C.2) by

$$H\overline{f}_r(x) - H\overline{f}(x) = \phi * \tilde{\lambda}(x) \text{ for } x \in (\overline{a}, \overline{e}) \text{ for some } |\tilde{\lambda}(x)| < 2\epsilon \text{ for } x \in (a, e).$$
 (C.5)

To replace (C.3), we use the second bound in (C.1) and the fact that $R\mu(s_0, \alpha_0) = \int_{\mathbb{R}} f(y) dy = \int_{\mathbb{R}} \overline{f}(y) dy$ to obtain

$$\left| \int_{\mathbb{D}} \overline{f}_r(y) \, \mathrm{d}y - \int_{\mathbb{D}} \overline{f}(y) \, \mathrm{d}y \right| \leqslant 2\epsilon. \tag{C.6}$$

Now we use (C.5) and (C.6) to prove (C.4). Recalling the definition of \overline{h}_1 and $\overline{h}_{1,r}$ (with the corresponding substitutions in formula (4.1)), we have

$$|\overline{h}_{1,r}(x) - \overline{h}_{1}(x)| \leq \frac{1}{\pi} \left| \int_{\mathbb{R}} \overline{f}_{r}(y) \, \mathrm{d}y - \int_{\mathbb{R}} \overline{f}(y) \, \mathrm{d}y \right| + \left| \frac{1}{\pi} \mathrm{p.v.} \int_{\overline{a}}^{\overline{e}} \frac{\mathrm{H} \overline{f}_{r} - \mathrm{H} \overline{f}(y)}{x - y} \sqrt{1 - y^{2}} \, \mathrm{d}y \right|$$

$$\leq \frac{2\epsilon}{\pi} + \left| \frac{1}{\pi} \mathrm{p.v.} \int_{\overline{a}}^{\overline{e}} \frac{\phi * \tilde{\lambda}(y)}{x - y} \sqrt{1 - y^{2}} \, \mathrm{d}y \right|$$
(C.7)

and we are left to bound $\left|\frac{1}{\pi}\text{p.v.}\int_{\overline{a}}^{\overline{e}}\frac{\phi*\tilde{\lambda}(y)}{x-y}\sqrt{1-y^2}\,\mathrm{d}y\right|$. Let us write $\sqrt{1-y^2}=\sqrt{1-x^2}+\kappa(y,x)$ with $\kappa(y,x):=(\sqrt{1-y^2}-\sqrt{1-x^2})$; then

$$\left| \frac{1}{\pi} \text{p.v.} \int_{\overline{a}}^{\overline{e}} \frac{\phi * \tilde{\lambda}(y)}{x - y} \sqrt{1 - y^2} \, dy \right| \leqslant \sqrt{1 - x^2} \left| \frac{1}{\pi} \text{p.v.} \int_{\overline{a}}^{\overline{e}} \frac{\phi * \tilde{\lambda}(y)}{y - x} \, dy \right| \tag{C.8}$$

$$+ \left| \frac{1}{\pi} \text{p.v.} \int_{\overline{a}}^{\overline{e}} \frac{\phi * \tilde{\lambda}(y)}{y - x} \kappa(x, y) \, dy \right|. \tag{C.9}$$

In order to bound (C.9), we observe that $\sup_{y \in (\overline{a}, \overline{e})} |\phi * \tilde{\lambda}(y)| \leq \sup_{y \in (a, e)} |\tilde{\lambda}(y)| \leq 2\epsilon$, that $\sup_{(y,x) \in [\overline{a}, \overline{e}] \times [\overline{a}, \overline{e}]} \left| \frac{\kappa(y,x)}{x-y} \right| =: C_1 < \infty$ and that $(\overline{a}, \overline{e}) \subset (-1, 1)$; hence,

$$\left| \frac{1}{\pi} \text{p.v.} \int_{\overline{a}}^{\overline{e}} \frac{\phi * \tilde{\lambda}(y)}{y - x} \kappa(x, y) \, dy \right| \leqslant \frac{4C_1 \epsilon}{\pi}. \tag{C.10}$$

In order to bound the right-hand side of (C.8), let us define $G : \mathbb{R} \to \mathbb{R}$ as

$$G(x) := \begin{cases} \tilde{\lambda}(x) & \text{for} \quad x \in (a, e) = (\overline{a} - \delta, \overline{e} + \delta) \\ 0 & \text{otherwise.} \end{cases}$$

We have the following properties for G:

$$\phi * G(x) = \phi * \tilde{\lambda}(x) \text{ for } x \in (\overline{a}, \overline{e})$$
 (C.11)

$$\sup_{x \in \mathbb{R}} |\phi * G(x)| \le 2\epsilon \tag{C.12}$$

$$\operatorname{supp}(\phi * G) \subset (-1, 1) \tag{C.13}$$

$$[H(\phi * G)](x) = [(H\phi) * G](x).$$
 (C.14)

Since $\phi \in C_0^{\infty}(\mathbb{R})$, we have that $H\phi \in C^{\infty}(\mathbb{R})$ and $H\phi(x) \to 0$ as $|x| \to \infty$. Hence, $\sup_{x \in \mathbb{R}} |H\phi(x)| =: C_2 < \infty$ and C_2 depends only on ϕ . With (C.12)–(C.14), this implies

$$|H(\phi * G)(x)| = |(H\phi) * G(x)| \le C_2 \int_{\mathbb{R}} |G(y)| dy = \le 4C_2 \epsilon.$$
 (C.15)

For $x \in (\overline{a}, \overline{e})$, we use (C.12) to compute directly that

$$\left| \frac{1}{\pi} \text{p.v.} \int_{(-1,\overline{a}) \cup (\overline{e},1)} \frac{\phi * G(y)}{y - x} \, dy \right| \leq \frac{1}{\pi} \int_{(-1,\overline{a}) \cup (\overline{e},1)} \frac{2\epsilon}{|y - x|} \, dy$$

$$= \frac{2\epsilon}{\pi} \left(\ln \left(\frac{x+1}{x - \overline{a}} \right) + \ln \left(\frac{1-x}{\overline{e} - x} \right) \right). \tag{C.16}$$

Using (C.11) and inequalities (C.15) and (C.16), we conclude that for $x \in (\overline{a}, \overline{e})$

$$\sqrt{1-x^2} \left| \frac{1}{\pi} \text{p.v.} \int_{\overline{a}}^{\overline{e}} \frac{\phi * \tilde{\lambda}(y)}{y-x} \, dy \right| \leq \left| H(\phi * G)(x) - \frac{1}{\pi} \text{p.v.} \int_{(-1,\overline{a}) \cup (\overline{e},1)} \frac{\phi * G(y)}{y-x} \, dy \right| \\
\leq \epsilon \left[4C_2 + \frac{2}{\pi} \left(\ln \left(\frac{x+1}{x-\overline{a}} \right) + \ln \left(\frac{1-x}{\overline{e}-x} \right) \right) \right]. \tag{C.17}$$

Finally, putting together (C.7), (C.10) and (C.17) we conclude that for $x \in (\overline{a}, \overline{e})$,

$$|\overline{h}_{1,r}(x) - \overline{h}_1(x)| \leqslant \frac{2\epsilon}{\pi} + \frac{4C_1\epsilon}{\pi} + \epsilon \left[4C_2 + \frac{2}{\pi} \left(\ln\left(\frac{x+1}{x-\overline{a}}\right) + \ln\left(\frac{1-x}{\overline{e}-x}\right) \right) \right]. \tag{C.18}$$

Let $C = \frac{2+4C_1}{\pi} + \left[4C_2 + \frac{2}{\pi}\left(\ln\left(\frac{\overline{b}+1}{\overline{b}-\overline{a}}\right) + \ln\left(\frac{1-\overline{c}}{\overline{c}}\right)\right)\right]$, defining $\overline{\epsilon} := C\epsilon$, which is proportional to ϵ . Let $\overline{E}(x) = \frac{1}{C}\left\{\frac{2+4C_1}{\pi} + \left[4C_2 + \frac{2}{\pi}\left(\ln\left(\frac{x+1}{x-\overline{a}}\right) + \ln\left(\frac{1-x}{\overline{c}-x}\right)\right)\right]\right\}$, which is continuous in $(\overline{a}, \overline{e})$ with $0 \le E(x) \le 1$ for $x \in (\overline{b}, \overline{c})$. Then (C.18) corresponds exactly to

$$|\overline{h}_{1,r}(x) - \overline{h}_1(x)| \leqslant \overline{\epsilon} \overline{E}(x).$$
 (C.19)

References

- [1] Ablowitz M J and Fokas A S 2003 Introduction and Applications of Complex Variables 2nd edn (Cambridge: Cambridge University Press)
- [2] Berenstein C A and Gay R 1991 Complex Variables, An Introduction (New York: Springer)
- [3] Clackdoyle R, Defrise M, Noo F and Kudo H 2006 Two-Dimensional Region-of-interest Tomography Oberwolfach Reports vol 3 ed G-M Greuel and S Klaus pp 2070–4
- [4] Clackdoyle R, Noo F, Guo J and Roberts J A 2004 Quantitative reconstruction from truncated projections in classical tomography IEEE Trans. Nucl. Sci. 51 2570–8
- [5] Clackdoyle R and Noo F 2004 A large class of inversion formulas for the 2D Radon transform of functions of compact support *Inverse Problems* 20 1281–91
- [6] Cormack A M 1963 Representation of a function by its line integrals, with some radiological applications J. Appl. Phys. 34 2722–7
- [7] Courdurier M 2007 La transformada de Rayos X: El problema interior con conocimiento a priori Seminario at Centro de Modelamiento Matematico (Santiago, Chile), available at www.cmm.uchile.cl/index.php?option=seminar&lang=en&m=1&v=2007
- [8] Courdurier M 2007 Image reconstruction from limited angle tomographic data with a priori knowledge Symp. on Inverse Problems Honoring Alberto Calderón (Rio de Janeiro, Brazil), available at http://www.math. purdue.edu/~sabarre/Calderon/parallel.html
- [9] Courdurier M 2007 Solving the interior problem of computerized tomography using a priori knowledge Applied Mathematics Colloquium at APAM (Columbia University), available at http://www.apam.columbia.edu/misc-pages/AM_2006-2007.html
- [10] Courdurier M 2007 Solving the interior problem in computerized tomography using a priori knowledge Conference on Applied Inverse Problems 2007: Theoretical and Computational Aspects (http://www.pims.math.ca/science/2007/07aip/abstracts.html)
- [11] Defrise M, Noo F, Clackdoyle R and Kudo H 2006 Truncated Hilbert transform and image reconstruction from limited tomographic data *Inverse Problems* 22 1037–53
- [12] Gelfand I M and Graev M I 1991 Crofton's function and inversion formulas in real integral geometry Funct. Anal. Appl. 25 1–5
- [13] Greenleaf A and Uhlmann G 1989 Non-local inversion formulas in integral geometry Duke J. Math. 58 205-40
- [14] Hamaker C, Smith K T, Solomon D C and Wagner S L 1980 The divergent beam X-ray transform *Rocky Mt. J.*

- [15] Helgason S 1999 The Radon Transform 2nd edn (Boston: Birkhäuser)
- [16] Katsevich A I and Ramm A G 1996 The Radon Transform and Local Tomography (Boca Raton, FL: CRC Press)
- [17] Kudo H 2006 Analytical image reconstruction methods for medical tomography—recent advances and a new uniqueness result *Proc. of Mathematical Aspects of Image Processing and Computer Vision 2006*, available at http://eprints.math.sci.hokudai.ac.jp/archive/00001652
- [18] Kudo H, Courdurier M, Noo F and Defrise M 2008 Tiny a priori knowledge solves the interior problem in computed tomography *Phys. Med. Biol.* 53 2207–31
- [19] Louis A K 1985 Incomplete data problems in X-ray computerized tomography: I. Singular value decomposition of the limited angle transform *Numer. Math.* 48 251–62
- [20] Louis A K and Rieder A 1989 Incomplete data problems in X-ray computerized tomography: II. Truncated projections and region-of-interest tomography *Numer. Math.* 56 371–83
- [21] Maass P 1992 The interior radon transform SIAM J. Appl. Math. 52 710-24
- [22] Natterer F 1986 The Mathematics of Computerized Tomography (New York: Wiley)
- [23] Noo F, Clackdoyle R and Pack J D 2004 A two-step Hilbert transform method for 2D image reconstruction Phys. Med. Biol. 49 3903–23
- [24] Pack J D, Noo F and Clackdoyle R 2005 Cone-beam reconstruction using the backprojection of locally filtered projections IEEE Trans. Med. Imaging 24 70–85
- [25] Quinto E T 1985 Singular value decomposition and inversion methods for the exterior Radon transform and a spherical transform J. Math. Anal. Appl. 95 437–48
- [26] Quinto E T 1993 Singularities of the X-ray transform and limited data tomography in \mathbb{R}^2 and \mathbb{R}^3 SIAM J. Math. Anal. 24 1215–25
- [27] Söhngen H 1937 Die Lösungen der integralgleichung $g(x) = \frac{1}{2\pi} \int_{-a}^{a} \frac{f(\xi)}{x-\xi} d\xi$ und deren Anwendung in der Tragflügeltheorie *Math. Z.* **45** 245–64
- [28] Tricomi F G 1957 Integral Equations (New York: Dover)
- [29] Ye Y, Yu H, Wei Y and Wang G 2007 A general local reconstruction approach based on a truncated Hilbert transform Int. J. Biomed. Imaging 2007 art-ID 63634
- [30] Ye Y, Yu H and Wang G 2007 Exact interior reconstruction with cone-beam CT Int. J. Biomed. Imaging 2007 art-ID 10693
- [31] Ye Y, Zhao S, Yu H and Wang G 2005 A general exact reconstruction for cone-beam CT via backprojectionfiltration IEEE Trans. Med. Imaging 24 1190-98
- [32] Zhuang T, Leng S, Nett B E and Chen G-H 2004 Fan-beam and cone-beam image reconstruction via filtering the backprojection image of differentiated projection data *Phys. Med. Biol.* 49 5489–503
- [33] Zou Y and Pan X 2004 Exact image reconstruction on PI-lines from minimum data in helical cone-beam CT Phys. Med. Biol. 49 941–59
- [34] Zou Y and Pan X 2004 An extended data function and its generalized backprojection for image reconstruction in helical cone-beam CT Phys. Med. Biol. 49 N383
- [35] Zou Y, Pan X and Sidky E Y 2005 Image reconstruction in regions-of-interest from truncated projections in a reduced fan-beam scan Phys. Med. Biol. 50 13–28